

15

VALVE TO MYOCARDIUM TENSION MEMBERS DEVICE AND METHOD

10

Background of the Invention

F

The present invention pertains generally to the field of heart valve repair. More specifically, the present invention 5 pertains to a device and method for the reduction of myocardial wall tension and the repair of mitral valve insufficiency.

Dilated cardiomyopathy is often accompanied by mitral valve insufficiency. There are several reasons for the 10 presence of mitral valve insufficiency associated with a dilated heart. First, chamber dilation and associated high wall stresses increase the diameter of the mitral valve annulus. Additionally, as the heart dilates, the positioning of the papillary muscles is altered. Papillary muscles and 15 chordae in a dilated heart will have moved both radially away and down from the mitral valve. This rearrangement of the vascular apparatus and enlargement of the annulus prevent the valve from closing properly.

Currently mitral valve insufficiency is treated by either 20 repairing or replacing the valve. Surgical procedures used to repair the valve including ring posterior annuloplasty which consists of sewing a C or D-shaped ring around the posterior leaflet of the mitral valve and drawing in the annulus, reducing its previously enlarged diameter. Another method is 25 to approximate the anterior and posterior mitral leaflets (Alfieri repair) by placing one suture through the center of both leaflets. This gives the valve a figure 8-shaped

appearance when the valve is opened. When the mitral valve is replaced, the original leaflets are removed and the chordae are cut. An artificial valve consists of mechanical or tissue leaflets suspended on struts attached to a metal stent, and is 5 sutured into place on the mitral annulus.

chsc 7

It has been argued that valve repair is preferable to valve replacement if the leaflet-chordae-papillary connections can be maintained. Heart wall stress will increase if the chordae are cut during valve replacement. It has been shown 10 that by severing the chordae there can be 30 percent (30%) reduction in chamber function. Mitral valve replacement has high mortality in very sick, chronic heart failure patients.

Summary of the Invention

15 The present invention pertains to a device and method for mitral valve repair. The mitral valve is generally defined as its leaflets or cusps, but in reality, it actually consists of the entire left ventricle chamber. By creating an improved chamber geometry, both chamber and valve function will be 20 improved. The device of the present invention and method for valve repair/replacement can include treatment for chronic heart failure by reducing left ventricular wall tension.

In one embodiment of the present invention, the valve repair device includes an elongate tension member having a 25 first end and second end. The basal anchor is disposed at the

first end and the secondary anchor is disposed at the second end.

The basal anchor could include a pad and annuloplasty ring or the like. Alternately an artificial heart valve could 5 serve as the basal anchor.

Tension members can be substantially rigid or substantially flexible. The secondary anchor can include a hook-shaped papillary muscle tissue loop, screw-shaped tissue anchor or transmural anchor pad.

10 The method of the present invention providing a tension member having a first end and a second end. The tension member has a basal anchor at the first end and a secondary anchor at the second end. The basal anchor is anchored proximate to the valve such that the tension member is 15 disposed in the chamber. The secondary anchor is anchored to a portion of the heart spaced from the basal anchor such that the tension member is under tension and the geometry of the chamber has been altered by placement of the tension member.

The basal anchor can include an artificial heart valve, 20 annuloplasty ring or the like. The secondary anchor can be anchored to a papillary muscle or transmurally anchored.

More than one tension member can be used. Additionally, a transverse tension member can be placed across the chamber generally perpendicular to the other tension members to 25 further alter the geometry of the heart, reducing wall stress and improving chamber performance.

Brief Description of the Drawings

Figure 1 is a transverse cross section of the left ventricle of a human heart taken from Figure 2;

Figure 2 is a vertical cross section of the left 5 ventricle of a human heart;

Figure 3 is a modified, transverse, cross section of the left ventricle of a human heart taken from Figure 4;

Figure 4 is modified, vertical cross section of a human heart, modified by a device in accordance with the present 10 invention;

Figure 5 is a cross section of an insufficient mitral valve of a left ventricle of a human heart;

Figure 6 is a cross section of a repaired valve and device in accordance with the present invention;

15 Figure 7 is an embodiment of the device of the present invention;

Figure 8 is an alternate embodiment of a device in accordance with the present invention;

Figure 9 is yet another alternate embodiment of a device 20 in accordance with the present invention;

Figure 10 is yet another alternate embodiment of the device in accordance with the present invention;

Figure 11 is yet another alternate embodiment of a device in accordance with the present invention;

25 Figure 12 is a view of a basal anchor for the device of the present invention;

Figure 13 is a suture ring serving as a basal anchor for the device of the present invention;

Figure 14 is a replacement valve serving as a anchor for the device of the present invention;

5 Figure 15 is a top view of an alternate embodiment of a suture ring acting as an anchor for the device of the present invention;

Figure 16 is a side view of the suture ring of Figure 15;

10 Figure 17 is a view of an alternate embodiment of a suture ring which can act as basal anchor for the device of the present invention;

Figure 18 is a view of yet another alternate embodiment of a suture ring which can act as a basal anchor for the present invention;

15 Figure 19 is a embodiment of a secondary anchor for the device of the present invention;

Figure 20 is a view of an alternate embodiment of a secondary anchor for the device of the present invention; and

20 Figure 21 is yet another embodiment of a secondary anchor for the device of the present invention.

Detailed Description of the Invention

Referring now the drawings wherein like reference
25 numerals refer to like elements throughout the several views,
Figure 1 shows a transverse cross section of the left

ventricle 10 of a failing heart taken from Figure 2. The papillary muscles 12 are shown in cross section. Figure 2 is a vertical cross section of human heart 10. A mitral valve is disposed near the top of left ventricle 10. Mitral valve 14 5 includes two leaflets or cusps 16. Chordae 18 extend between leaflets 16 and papillary muscles 12.

Figure 3 is a cross section of heart 10 modified from that shown in Figure 1 by placement of valve repair device 20 in accordance with the present invention as shown in Figure 4. 10 Figure 4 is a vertical cross section of left ventricle 10 with geometry modified by device 20. In this embodiment of the invention, device 20 includes a basal anchor 22 such as an annuloplasty or suture ring sewn proximate the annulus of valve 14. Extending from basal anchor 22 are elongate tension 15 members 24. Each have a first end connected to basal anchor 22 and a second end anchored to papillary muscles 12 or the heart wall.

As can be seen in Figures 3 and 4, both the transverse radius and vertical dimension of left ventricle 10 has been 20 reduced in comparison to that of Figures 1 and 2 by drawing papillary muscles 12 toward valve 14 with tension members 24. This change in geometry reduces heart wall stress and consequently increasing chamber function. Valve function is also improved as explained in more detail by reference to 25 Figures 5 and 6.

Figure 5 is a generally vertical cross section of an insufficient mitral valve of a heart suffering from chronic heart failure. In this case as the failing heart has dilated, papillary muscle 12 has been drawn away from mitral valve 14.

5 The chordae connections between papillary muscles 12 and valve 14 in turn draws leaflets 16 apart such that during the normal cardiac cycle, leaflets 16 may not completely close. Thus, an opening 26 is left between leaflets 16 throughout the cardiac cycle. Opening 26 will allow blood to leak, reducing chamber 10 efficiency.

Figure 6 is a view of the mitral valve 14 of Figure 5 which has been modified by placement of valve repair device 20 as shown. Suture ring 22 is sewn proximate the annulus of valve 14, as known to those skilled in the use of suture 15 rings. The annulus of valve 14 can be decreased in size by drawing the annulus toward the suture ring by the sutures used to connect ring 22 to the valve. Drawing the annulus of valve 14 toward suture ring 22 will help to eliminate opening 26. Tension member 24 is then anchored to papillary muscle 12 such 20 that papillary muscle 12 is drawn toward valve 14. Whether or not the suture ring alone is sufficient to eliminate opening 26, drawing papillary muscle 12 toward valve 14 will provide additional stress relief on leaflet 16 promoting complete closure of valve 14. Drawing papillary muscle 12 toward 14 25 also reduces heart wall stress and increases chamber efficiency as discussed previously.

Figure 7 is a highly simplified view of left ventricle 10 and valve repair device 20 as shown in Figure 4. It can be noted that tension members 24 extend from basal anchor 22 to an adjacent papillary muscle 12. In contrast, Figure 8 is a 5 similar cross sectional view of left ventricle 10, but a valve repair device 120 is placed such that its tension members 124 extend between a basal anchor 122 and a papillary muscle 12 transversely opposite the point at which tension member 124 is connected to basal anchor 122. This arrangement, as opposed 10 to that shown in Figure 7, can increase the transverse component of the tension force in tension members 124 relative to the vertical component of that tensile force.

Figure 9 shows yet another embodiment of the valve repair device in accordance with the present invention referred to by 15 numeral 220. In this embodiment, device 220 is disposed in left ventricle 10 in a manner similar to that of device 20 shown in Figure 7 in that tension members 224 of device 220 extend from a basal anchor 222 to an adjacent secondary anchor point. The secondary anchor point is established by 20 transverse extension of a tension member 225 across left ventricle 10. Tension member 225 is anchored transmurally to the heart wall at its opposite ends by pads 227. In turn, tension members 224 are anchored or connected to tension member 225.

25 Tension member 225 can be used to further alter the geometry of left ventricle 10 in a manner disclosed in U.S.

Patent Application Serial No. 08/933,456, entitled "HEART WALL TENSION REDUCTION APPARATUS AND METHOD", which was filed on September 18, 1997 and is incorporated herein by reference.

Figure 10 shows yet another embodiment of a valve repair device in accordance with the present invention referred to by numeral 320. This embodiment includes a basal anchor 322 and tension members 324 and a transverse tension member 325 having anchor pads 327 similar to those of device 220. With respect to device 320, however, tension members 324 are crossed similar to those of device 120 of Figure 8 to increase the horizontal component relative to the vertical component of the tensile force in tension member 324.

Figure 11 is a yet another embodiment 420 of the valve repair device of the present method. Valve repair device 420 includes a basal anchor 422 and tension members 424. Tension members 424 are disposed in an arrangement similar to tension members 24 of device 20 shown in Figure 7 except that tension members 424 are anchored transmurally by pads 427 rather than into papillary muscles 12. The relatively greater thickness of tension members 424 shown in Figure 11, as compared to tension members 24 shown in Figure 7, merely illustrates that the tension members can be substantially rigid or in the case of tension members 24, substantially flexible. It should be understood, however, that in any of the embodiments shown herein, the tension members could be advantageously formed to be substantially flexible or substantially rigid.

Figure 12 is a top or posterior view of valve 14. In this embodiment, the basal anchor for the valve repair device is shown as discrete pads 28 which can be sewn to the posterior side of valve 14. Tension members 24 are shown 5 extending from respective pads 28 into the left ventricle.

Figure 13 is the same view of valve 14 as Figure 12. In Figure 13, however, the basal anchor 22 is shown as a crescent-shaped suture ring. Tension members 24 extends from basal anchor 22 through valve 14 into the left ventricle.

10 Figure 14 is a side view of an artificial heart valve 30. If it is necessary to replace the valve rather than merely repair it, artificial valve 30 can be used as a basal anchor for tension members 24.

15 Figure 15 is a top view of an alternate embodiment of a suture ring basal anchor 32. Ring 32 has a crescent shape and a pylon 34 extending through the mitral valve. Figure 16 is a side view of suture ring 32 showing tension members 24 attached to pylon 34.

20 Tension members 24 preferably extend through the tissue of valve 14 rather than through the valve opening. It can be appreciated, however, that tension members 24 could be disposed through the valve opening. In the case of the embodiment of Figures 15 and 16, however, pylon 34 would be disposed through the valve opening. Tension members 24 25 associated with pylon 34 would be disposed on the opposite side of valve 14 from suture ring 32. Pylon 34 would

preferably be disposed through the valve opening rather than the tissue forming valve 14.

Figures 17 and 18 are yet additional alternate embodiments of suture rings which can be used as basal anchors 5 in accordance with the present invention. The shape of the rings is selected such that as they are sewn into place on valve 14, the sutures can be used to draw tissue toward the inside of the ring, thus reducing the transverse and/or vertical cross sectional area of the associated heart chamber. 10 This will advantageously reduce heart wall stress which is of particular benefit if the patient has a failing heart.

It can be appreciated that tension members 24 can be fixably or releasably attached to the basal anchor. Preferably, the tension members are fixably attached to the 15 basal anchor during the valve repair procedure.

Figures 19-21 show various configurations of anchoring devices shown at the second end of tension member 24. It can be appreciated that these anchoring devices could be used with each of the tension members described above. In Figure 19, the 20 second end of tension member 24 includes a secondary anchor 40 formed as screw which is shown augured into papillary muscle 12. Figure 20 shows a secondary anchor 42 including a loop sewn through papillary muscle 12. Figure 21 shows a tension member 24 extending transmurally to an exterior pad 44 to 25 which it is connected. Tension member 24 could be sewn to pad 44 or otherwise mechanically connected thereto.

It can be appreciated that various biocompatible materials can be advantageously used to form the various components of the device of the present invention. It is anticipated that the present device will usually be 5 chronically implanted. Thus, when selecting materials to form each of the components consideration should be given to the consequences of long term exposure of the device to tissue and tissue to the device.

Numerous characteristics and advantages of the invention
10 covered by this document have been set forth in the foregoing
description. It will be understood, however, that this
disclosure is, in many respects, only illustrative. Changes
may be made in details, particularly in matters of shape,
size, and arrangement of parts without exceeding the scope of
15 the invention. The invention's scope is, of course, defined
in the language in which the appended claims are expressed.